1	Experimental and simulated evaluation of airborne
2	contaminant exposure in a room with a modified localized
3	laminar airflow system
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16

17 Abstract:

18 The traditional mixing ventilation is not an energy effective approach to remove indoor 19 air pollutants, maintain breath zone air quality, and control the airborne transmission. 20 This study investigated the potential of a localized laminar airflow ventilation system 21 to alleviate human exposure to pollutants. Breathing thermal manikins with sitting 22 posture and supine posture were used to simulate the human. N₂O was used as the tracer 23 gas to simulate the indoor pollutants emission. The contaminant exposure index (ε_{exp}) 24 and intake fraction index (IF) were used to assess the risk of human pollutant exposure for various supply air velocities given different emission source positions. Enhanced 25 26 pollutant removal efficiency (E_{ff}) (from the result) showed the qualification and 27 desirability of the localized laminar airflow ventilation system in improving the breath 28 zone air quality. The results showed that the CFD results could fit well with the 29 experimental data, and found out the interaction between thermal plume and supply air. The results also indicated a low ε_{exp} and IF, with the Eff over 90%, all of which were 30 31 highly correlated with the supply velocity. Human's different breathing methods have 32 little influence on the pollutant exposure so as to the location of the pollution source. 33 This study found that localized laminar airflow ventilation system could efficiently

- 34 provide fresh air to the breathing zone without sacrificing the thermal environment
- around human. It can be used for small region air quality control such as that in the
- 36 bedroom and living room where desired air quality is favored.
- 37 Key words: localized laminar airflow system; breathing thermal manikin; pollutant
- 38 exposure; pollutant removal efficiency.

39 1. Introduction

40 Human spend over 80% of their lifetime in the indoor environment (Dodson et al. 41 2007) and about two-thirds of a day inside their houses or dwellings (Zhang et al. 2009). 42 Nowadays, study on ventilation problems in residential buildings has been conducted (Kyoungbin et al. 2008; Richard et al. 1997; Vernon et al. 1997), but, the some scholars 43 44 focused on the kitchen space. A more recent study (Cheng et al. 2018) further 45 investigated people's time distribution in residence and found people spend near 85% 46 of their time in the living room and bedroom of which bedroom alone could take up 55% 47 of the time. Thus, people's health risk from the indoor pollutant exposure could be 48 greatly reduced if we can take control over the air quality of the bedroom and living room, which also means an improvement in people's living environment. In addition, 49 50 there are several critical considerations that make these two environments (i.e., the 51 bedroom and living room) unique: (1) the prolonged period of exposure due to sleeping time, which makes up nearly one third of people's lives in the bedroom (Dodson et al. 52 53 2007; Zhang et al. 2009); (2) the potential for higher exposure due to people's closer 54 proximity to the breathing zone (BZ) pollutant sources; and (3) the existence of 55 diversified indoor pollutants such as gaseous-phase contaminants.

Air-conditioning systems were commonly used for the indoor environment control and thermal comfort management in the residential buildings. Ventilation is increasingly becoming recognised as an important component of a healthy residential building, and is the ultimate strategy to control indoor air quality (IAQ) (Dimitroulopoulou, 2012). For the requirements of ventilating flow rates, energy 61 consumption and IAQ would have conflict, and thermal comfort would also be affected by the ventilating flow rates (Kim et al, 2009; Lozinsky et al. 2020). However, 62 63 traditional air-conditioning systems typically mix the clean, filtered air with the ambient room air and return air. As a result of this mixing effect, the pollutants concentration of 64 65 the BZ air almost equals to the concentration of the mixed air. Moreover, the strong 66 supply airflow draft could deliver the near-surface pollutants (such as those on/near the 67 furniture surfaces) to the BZ (Spilak et al. 2016), which is another critical air quality consideration of the traditional systems. On the other hand, portable air cleaners (also 68 69 known as air purifiers) are often used in homes and offices due to their high particle-70 removal efficiencies, no need of pre-installations and relative low prices (Spilak et al. 71 2014; Bräuner et al. 2008). However, the filtered air from the portable air cleaner will 72 be mixed with the indoor air in a similar way as that of the traditional heating, ventilation, and air conditioning (HVAC) systems. Hence, the portable air cleaners 73 could have the same BZ air quality considerations as that of the HVAC systems. 74

75 Recently, the temperature-controlled laminar airflow (TLA) has been investigated 76 by some researchers as an indoor environment control alternative in the health care 77 systems (Spilak et al. 2016; Pedroletti et al. 2009; Evans et al. 2010). The TLA 78 environment control approach relies on a local downward laminar airflow, which 79 delivers low-speed air via overhead supply nozzles after the air been filtered, cleaned and conditioned. The cooler air supplied by the TLA system flows downward against 80 81 the upward convection airflows that caused by the thermal plumes of the sitting and/or 82 sleeping person. Since the supply air is delivered locally to the BZ, the mixing effect

with the indoor air is greatly reduced, resulting in a significantly lower amount of
supply air required by the BZ to achieve the same air quality and/or thermal comfort as
required by the traditional HVAC systems or portable air cleaners (Cong et al. 2018).

Nowadays, the laminar airflow (LAF) has been proven by many scholars as an 86 better airflow to maintain clean air compared to the mixing airflow approach, it has 87 88 been widely applied for the hospitals' air systems to reduce the patients' exposure risk to particles (Lidwell et al. 1982; Memarzadeh et al. 2002; Chow et al. 2004; Oguz et al. 89 90 2017; Whyte et al. 1982; Hirsch et al. 2012; Diab-Elschahawi et al. 2011; Fischer et al. 91 2015). In addition, LAF systems are commonly used to remove airborne microbial 92 particles and other pollutants in hospital operation room or other places where strict indoor environment are required. 93

94 Some scholars focused on the efficiency of the TLA system used for diseases risk control and management. In a study, a bedside device using horizontal laminar airflow 95 96 was introduced to alleviate rhinitis symptoms and daytime somnolence (Morris et al. 97 2006). Another researcher introduced the TLA system to improve asthma-specific 98 quality of life and ease airways inflammation (Boyle et al. 2016). Some scholars 99 focused on the efficiency of TLA for particles removal. As a study showed, the 100 magnitude of the reduction was more than 99% in every category within 30 minutes by using TLA system (Gore et al. 2015). Another study showed the similar result, The TLA 101 102 device could remove the 99.9% of the initial particles in a short time and the downward 103 LAF was able to prevent the particles from peripheral zone move into the BZ, keep the BZ air quality isolate from peripheral zone (Spilak et al. 2016). A scholar compared 104

105 real-person exposure in bed with two different cases, and it obtained the similar results with previous studies (Gore et al. 2015). There was a research considered both decease 106 107 and particle, TLA system achieved massive reductions in both total particle and cat allergen concentrations in the BZ while subject lying on the bed (Warner et al. 2017). 108 109 According to these studies, TLA could remove over 99% airborne particles of all sizes, 110 and the concentrations of particles outside the TLA airflow zone did not change, it 111 would have high concentration compared to the BZ (Warner et al. 2017). However, the supply air is supplied directly straight to the people, the thermal plume of the people 112 113 appears to have a greater effect on velocity field and temperature field in the LAF 114 system than in the traditional mixing ventilation system, the thermal plume may 115 decrease the supply air velocity which may cause the unstable situation in TLA airflow 116 zone, the pollutants might move into BZ. It could increase the exposure of the patient to various indoor airborne pollutants (Guangyu et al. 2019). A previous study taken 117 placed in hospital found that the location of the pollutant source may not be a significant 118 factor to affect the risk of exposure (Guangyu et al. 2019). 119

Although the TLA system was showed to be effective in improving the BZ air quality in the hospitals, the environment of the hospital is actually different from that of the residence (with respect to the pollutant source, number of people, and the cost of the TLA system). Thus, it is not reasonable to straightly apply the TLA system used in the hospitals for residences or for ventiate spaces for residential uses. In order to use the TLA system for residential buildings, the regular system used in the hospital may need to be modified. In this study, we draw lessons from past applications of the TLA

system, and make a modified and simplified version of TLA which is a localized or 127 personal LAF. And the main objective of this study is to experimentally and 128 129 simulatively determine pollutants exposure by assessing the risk of pollutants in a room with modified LAF system. To achieve this objective, we i) investigated the impact of 130 ventilation air flow velocities on the pollutants-removal effectiveness in the BZ, ii) 131 132 compared the impact of different emission sources locations on the pollutants-removal effectiveness in the BZ, iii) investigated the impact of different breathing modes on the 133 *E*_{ff} in the BZ. 134

135 **2. Methods**

136 *2.1. Test room and experimental setup*

137 The experiment was conducted in a small climate chamber, with a dimensions of 3.95m×2.35m×2.65m (L×W×H) as shown in Fig. 1. The air was supplied from a 0.50 138 139 $m \times 0.50$ m laminar air panel in the middle of the room positioned 2.2 m above the 140 floor. Compared with the traditional localized laminar systems used in hospitals, the nozzle outlet of the diffuser in this experiment was equipped with honeycomb flow 141 142 straighteners (Ø4 mm) to straighten the flow and to reduce the turbulence intensity. In addition, the system dimension was much smaller. The air was exhausted through two 143 exhaust outlets with opening areas of 0.0256m² located on the sidewall (Fig.1). During 144 the test, the room temperature was kept at $23.0 \pm 0.5^{\circ}$ C and frequently checked by the 145 146 temperature measurements from a TSI VelociCalc 9565-P multi-function ventilation 147 meter in the middle of the chamber with a height of 1.5m.





Figure 1 Schematic diagrams of the full-scale experiment ward (a)sitting case (b) supine case

157 *2.2. Simulation setup*

158 CFD simulations were performed with Ansys Fluent 19.1 (ANSYS, Inc.) using k-159 ε RNG turbulence model. The buoyancy force was obtained by Boussinesq 160 approximation, air density was treated to be constant during the calculation. No slip 161 and fixed temperature condition were given as the boundary condition for the body surface and wall. The gravitational acceleration (g) and the thermal expansion 162 coefficient (β) were 0.00333k⁻¹ and -9.8m/s² respectively. Surface temperature of 163 manikin's head was assigned to be 31 °C while other parts were 26.6 °C. Environmental 164 temperature was designed by defining floor, ceiling, wall, bed and chair temperature, 165 which was given as 23 °C. The density of surface of manikin was 1200kg/m³, specific 166 heat capacity and thermal conductivity were 3300j/kg/k and 0.34w/m/k respectively. 167 Density, specific heat capacity and thermal conductivity of the insulation wall were 168 1200kg/m³, 970j/kg/k and 0.17w/m/k respectively. The supply air velocity was different 169 170 in two different posture. For sitting model, the magnitude of velocity was 0.25m/s, 0.30m/s and 0.35m/s, for supine model, the magnitude of velocity was 0.15m/s, 171 172 0.25m/s, and 0.35m/s. K and Epsilon was 0.0001 and 0.00001 respectively. The exhaust was pressure outlet. 173

SIMPLE scheme was adopted for Pressure-velocity coupling Method. Power law
scheme was adopted for momentum equation and energy equation discretization.
PRESTO ! scheme was adopted for pressure interpolation schemes. Second-order
upwind differential was adopted for others. Parallel computing was conducted to
accelerate the calculation.

179 Calculation domain was divided into different parts for the mesh generation. Fine 180 grid was generated for the zones around human body and laminar air flow panel to 181 insure sufficient grid for the simulation need of thermal plume and supply air. The size 182 of the grid was from 2mm to 45mm. Moreover, size function was defined to refine the 183 grid on human body surface, laminar air flow panel and exhausts. For manikin, first 184 layer size in contact with body surface was 0.9mm considering a growth ratio of 1.1 185 with a total number of 6 layers. For other surfaces, first layer size was 4mm considering 186 a growth ratio of 1.1 with a total number of 8 layer. In sitting case, the totally 4.4 million 187 grids were defined for the calculation. In supine case, the totally 4.2 million grids were 188 defined for the calculation.

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Figure 2 Simulation model (sitting posture) (a)Chamber; (b)Mesh of manikin



Figure 3 Simulation model (supine posture) (a)Chamber; (b)Mesh of manikin

191 *2.3. Breathing thermal manikins*

Previous study showed that the use of the thermal manikins is a practical and 192 effective approach method to study the interaction between thermal plumes and the 193 downward laminar airflow (Guangyu et al. 2018). To simulate the human subject, a 194 195 breathing thermal manikin with a complex body shape was used. Two thermal manikins with performing an specific breathing function are used during the experiments. The 196 197 supine manikin was a 1.85m tall man while the sitting manikin was a 1.7m woman. The female manikin dressed in shirt and jeans with an insulation value of approximately 198 0.8clo and was seated on a cylinder which had a height of 0.48m to minimize the impact 199 of the chair on airflow distribution. The male manikin was placed on a 0.7m height and 200 201 0.6m width bed covered with the cotton-type sheet as the supine position covered with thin quilt below laminar air flow panel. 202

203

Table 1 Summary of the experiments with different parameters

Parameter	Conditions	Details/comments
Ambient	23±0.5°C	-
Manikin heat output	113W	33-34°C
	80W	
Body posture	Sitting	Upright
	lying	

190

Clothing	Thick loose clothing	Tight jeans, thick loose
		long-sleeve shirt
	Wig	Short hair wig, slightly
		below the ear level
Chair	Cylinder	0.48m height
Bed	Sheet	0.7m height and 0.6m width
Breathing	Mouth	See Table 2
	Nose	

The manikin's breathing system can simulate the realistic airflow associated with the human inhalation and exhalation. The detail information of the exhalation orifices and breathing function was shown in Table 2. The maximum exhalation air velocity is 3.7m/s at the mouth, and the temperature of the exhalation air is around 26°C. The use of artificial breathing device in the manikin was not used during the non-breathing measurements.

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211

212 **Table 2** Respiration parameters of the breathing thermal manikin.

Frequency of breathing	air flow	Mouth area	Nose area
(time/min)	(L/min)	(cm^2)	(cm^2)
17.5	8.61	1.20	0.70

213 *2.4. Tracer gas (N₂O) setup and instruments*

Nitrous oxide (N₂O) was used as the tracer gas to simulate the pollutant. During
the experiment, the N₂O was continuously released by a tube (Ø33 mm) with the gas

flowrate of controlled at 0.40L/min. The tracer gas was successively sampled by four
plastic tubes placed at 4 different locations (in the BZ, at the supply air panel, and at
the two exhausts). The sampled tracer gas was then sent to a pre-calibrated Innova 1303
multi-gas sampler and doser (Brüel & Kjær, Ballerup, Denmark) coupled to an Innova
1302 photo-acoustic monitor.





(a)

(0)

Figure 4 Tracer gas system (a) Trace detector (b) Gas cylinder

221	The performance of the anemometer system are shown in Table 3. The air velocity
222	measurement system was "AirDistSys5000 (Sensor-electronic inc.). The system has 3
223	part: (1)a pressure sensor which is used to correct the anemometer readings according
224	to the barometric pressure, (2)five omnidirectional anemometer probes, (3)a wireless
225	transmitter transmitting the readings to a USB interface which is connected to a
226	computer and to a power supply.

 Table 3 Parameters of the air velocity measurement system.

Model	Measuring variable	Range	Accuracy	Resolution
SensoAnemo5100LSF	Velocity	0.05-5m/s	±0.02m/s or ±1.5% of readings	0.001m/s
SensoAnemo5100LSF	Temperature	-10°C-50°C	±0.2°C	0.1°C
SensoBar 5301	Pressure	500-1500hPa	±3hPa	lhPa

227 2.5. Contamination distribution indices

To investigate the pollutant remove efficiency of the modified LAF, only considering the efficiency is not enough. To make sure that the modified LAF system is functioning for residential purposes, in this study, exposure index is also considered.

The exposure to contaminants in the BZ of the manikin was determined using the local relative contaminant exposure index ε_{exp} . This indice has been used in a similar approach in previous studies (Cao et al. 2015; Berlanga et al. 2017; Olmedo et al. 2012). The contaminant exposure index ε_{exp} is defined as:

$$\varepsilon_{exp} = \frac{C_l - C_s}{C_{exh} - C_s} = \frac{C_l}{C_{exh}}$$
(1)

Where C_l is the average tracer gas concentration in the inhaled air of the receiving manikin and C_s and C_{exh} are the average tracer gas concentrations in the supply and exhausts respectively. The N₂O concentration of the supply air was assumed to be zero as the background concentration of N₂O was extremely low. A low contaminant exposure index means a low concentration of airborne pollutants in the experimental measurement point. To investigate the intake risk, the intake fraction (*IF*) index (Laverge et al. 2014)
was introduced. Its value is obtained as:

244
$$IF = \frac{\int Q_b C dt}{\int E dt}$$
(2)

Where *IF* is intake fraction, Q_b is the breathing rate of manikin (L/s). Where *C* is the concentration of the pollutant at the sampling site, which is equal to the C_l in equation 1. Being *E* the emission rate of the pollutant (L/s).

$$E_{ff} = \frac{c_{mix} - c_l}{c_l} \tag{3}$$

Where C_{mix} is the pollutant concentration in breathing zone with mixing ventilation, E_{ff} is the efficiency of removing the pollutant. In this equation, the modified localized laminar airflow system was regarded as a type of air cleaner, the E_{ff} is the same with the "Reduction effectiveness index" which was used to estimate the overall effectiveness of the air cleaners (Miller-Leiden et al. 1996; Spilak et al. 2016).

254 2.6. Investigated cases

255 The study consists of 5 experimental cases, based on the different supply air velocity and location of pollutant source, separated in 15 groups. Every group has two 256 257 experiments, mouth breathing mode experiment and nose breathing mode experiment. 258 The measurements are repeated in each group for three different velocities of the supply airflow: 0.15, 0.25 and 0.35 m/s for lying manikin, and 0.25, 0.30, 0.35 for sitting 259 260 manikin. The ventilation rate is from 5.4ACH to 12.8ACH with the supply air velocity is from 0.15m/s to 0.35m/s. All cases are summarized in Table 4. The placements of the 261 sampling and the pollutant source are shown in Fig. 5. 262

groups	posture	Supply air(m/s)	Pollutant source location
1		0.25m/s	1 m in front of the menilia
2		0.30m/s	
3		0.35m/s	(case 1)
4		0.25m/s	
5	Sitting	0.30m/s	Im side away from the manikin
6		0.35m/s	(case 2)
7		0.25m/s	Class to the healt well
8		0.30m/s	
9		0.35m/s	(case 3)
10		0.15m/s	1 m in front of the had
11		0.25m/s	Im in front of the bed
12	a .	0.35m/s	(case 4)
13	Supine	0.15m/s	0.5m away from the and of the had
14		0.25m/s	(2000 5)
15		0.35m/s	(case 3)

Table 4 Cases studied in this investigation.

263



Figure 5 Placement of sampling and pollutant source

264 3. Results and discussion

265 *3.1. Feasibility simulation*

To see whether the modified airflow system was suitable or not, it was necessary to perform the simulation. If the simulation results showed that the supply can not reach the breathing zone, the experiment had no meaning.

269 3.1.1 Sitting posture simulation results

As shown in Fig.6(a) and (b), when the supply air velocity was 0.25m/s, the situation of the supply air got in touch with the human thermal plume. However, the thermal plume covered the breathing zone. The supply air spread from the head. Fig.6(c) and (d) showed the vector distribution 5cm and 10cm distance away from the manikin. At 5cm distance, the supply air could reach the height of mouth, and at 10cm distance, the supply air could reach the height of neck. It was not enough to improve the air quality in breathing zone.

277





(b)



Figure 6 Vector distribution(0.25m/s) (a)Side view;(b) Central of manikin;(c) 5cm away;

(d)10cm away

278	In Fig.7, the magnitude of velocity could be seen very directly. In the side view,
279	the supply air velocity dropped dramatically from a certain height above the head.
280	Because of the thermal plume, the magnitude of velocity was very small close to the
281	head. The velocity near the face region was very small, and the direction was upward.
282	The distance of downward movement of supply air is limited, which could not achieve
283	the desired effect on restricting the role of thermal plume, and the effect of improving
284	the air quality in the breathing zone was limited.

285





Figure 7 Velocity distribution(0.25m/s) (a)Side view;(b) Central of manikin;

(c) 5cm away;(d)10cm away

As Fig.8 showed, when the supply air velocity was 0.30m/s, the vector distribution had difference with the supply air velocity was 0.25m/s. First, the supply air could reach even further. Then, when the supply air touched the head, the angle of diffusion narrows compared to the lower supply air velocity. Most important, the supply air could reach the breathing zone, the impact of thermal plume was limited. The air optimization effect should be better.

292





Figure 8 Vector distribution(0.30m/s) (a)Side view;(b) Central of manikin;(c) 5cm away;

(d)10cm away

In Fig.9, the magnitude of velocity near the face was bigger than the lower supply air situation. The supply air could reach the neck height. This supply air velocity could provide better air quality in breathing zone. The velocity around the manikin is near 0.2m/s, it has little influence on thermal comfort. The velocity will discuss in the next section.

298



(a)

(b)



Figure 9 Velocity distribution(0.30m/s) (a)Side view;(b) Central of manikin;

(c) 5cm away;(d)10cm away

299 Fig.10 and Fig.11 showed the velocity distribution when the supply air velocity increased to 0.35m/s. In the side view (Fig.9(a)), it was very similar with the lower 300 supply air velocity situations. The interaction between supply air and thermal plume 301 302 was a little bigger than lower supply air velocity situation. The angle of diffusion 303 narrows slightly. Meanwhile, the supply air could reach further distance in front the manikin. When the supply air was 0.35m/s, it might provide the best air quality in 304 breathing zone. However, when the supply air was relatively high, it might disturb the 305 306 pollutants near the floor. Also, the higher velocity might cause uncomfortable drafts 307 feelings.



(b)



Figure 10 Vector distribution(0.35m/s) (a)Side view;(b) Central of manikin;(c) 5cm away;

(d)10cm away

308	In Fig.11, the pollutant near the floor was disturbed because of the high supply air
309	velocity. This might have influence on the whole indoor environment. In addition, the
310	influence of air velocity on the thermal comfort should have bad impact.

311









(c)

Figure 11 Velocity distribution(0.35m/s) (a)Side view;(b) Central of manikin;

(c) 5cm away;(d)10cm away

312 3.1.2 Supine posture simulation results

(a)

- For the supine posture, breathing zone is the most important zone. In this section,
- 314 the velocity distribution was focused.
- As Fig.12 showed, when the supply air was 0.15m/s, the magnitude of velocity dropped rapidly near the surface of the head. And the vortex was generated near the face. The fresh air could not reach the face. Although, the 0.15m/s supply air could separate the breathing zone from other space, the low supply air could not provide as much as possible fresh air into the breathing zone.
- 320 Near the bed, the air could follow the thermal plume move to the breathing zone,
- which means that the pollutant near the bed might also move to the breathing zone, butit needs more detail research.



(b)



Figure 12 Vector distribution(0.15m/s) (a)Side view;(b)Philrum;(c)Forehead;(d)Neck

As Fig.13 showed, the velocity distribution presented that the velocity dropped 323 dramatically near the head. The 0.15m/s supply air velocity was not enough to provide 324 the high-quality air in breathing zone. The pollutant near head region would not move 325 away according to this figure. 326

327



(a)



Figure 13 Velocity distribution(0.15m/s) (a)Side view;(b)Philrum;(c)Forehead;(d)Neck

As Fig.14 showed, when the velocity increased to 0.25m/s, the fresh air could move directly near the face, also it could make the air near bed not move to the breathing zone. This velocity could change direction of the air around the head and let the breathing zone have high-quality air. The pollutant around the lower part of the manikin would not move into the breathing zone.

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Figure 14 Vector distribution(0.25m/s) (a)Side view;(b)Philrum;(c)Forehead;(d)Neck

The velocity distribution was very similar with the lower supply air velocity situation (Fig.15). This velocity has little impact on the air near the floor. The air above the manikin is downward and the velocity near head is around 0.15m/s, it has little impact on thermal comfort.

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Figure 15 Velocity distribution(0.25m/s) (a)Side view;(b)Philrum;(c)Forehead;(d)Neck

When the supply air was 0.35m/s, the interaction with thermal was the same with 339 0.25m/s supply air (Fig.16). However, above the lower part of the body, the air had 340 vortex, which means the pollutant could gather here and not move to the exhaust. 341







Figure 16 Vector distribution(0.35m/s) (a)Side view;(b)Philrum;(c)Forehead;(d)Neck

As fig.17 showed, the highest supply air velocity had impact on the air near the floor. The air was forced to move upwards, also the pollutant near the floor. For the whole environment, this velocity might not be the best choose. The velocity around head is around 0.2m/s, it has more impact on the thermal comfort compare to the lower supply air velocity.



Figure 17 Velocity distribution(0.35m/s) (a)Side view;(b)Philrum;(c)Forehead;(d)Neck

347

348 *3.2. Characteristic of the airflow above the manikin*

- 349 3.2.1 Sitting position
- 350 To investigate the characteristic of the airflow above the sitting manikin, there

were 6 sampling point located above the manikin. The sampling points placed at 5cm
horizontal distance away from the philtrum and forehead, and 10cm, 20cm, 30cm above
the head. The last point placed at supply air inlet.

354



Figure 18 Velocity at different position(a)Mouth breathing;(b)Nose breathing

As for sitting position experiment, the supply air had 3 different velocities, 0.25m/s, 0.30m/s and 0.35m/s respectively. The Fig.18 present the velocity above the manikin. The velocity distributions were very similar between mouth breathing case and nose breathing case, the change of the velocity value were almost the same.

359 With the sampling point height decrease, the velocity magnitude went down from 360 inlet to 10cm vertical distance from head. However, at the 5cm horizontal distance from 361 forehead, the magnitude of velocity changes drastically. When the supply air velocity 362 is 0.25m/s, because of the magnitude of the supply air velocity was small, the velocity 363 direction might have changed above the head which means that the velocity with small magnitude at philtrum and forehead height might had opposite direction with supply 364 air velocity, this phenomenon needs further study. When the supply air velocity was 365 0.30m/s or 0.35m/s, the velocity at forehead height increased dramatically which means 366

the supply had downward trend after contacting with head and the airflow could flow



369



Figure 19 Turbulence intensity at different position(a)Mouth breathing;(b)Nose breathing In Fig.19, when the supply air velocity was 0.25m/s, the airflow had big turbulence at 10cm vertical distance above the head. Because the human thermal plume had the impact on the supply air, the supply air with this magnitude can not deliver the clean air to the breathing zone. When the supply air velocity was 0.30m/s or 0.35m/s, the turbulence intensity increased slightly because of the shape of the head blocked the movement of supply air. At the height of philtrum, the turbulence intensity increased dramatically, because of the interaction of breathing air and supply air.

377 3.2.2 Supine position

To investigate the characteristic of the airflow above the supine manikin, there were also 6 sampling point located above the manikin's head. The sampling points placed above the philtrum, the distance were 5cm, 15cm, 25cm, 35cm and 45cm. The last point placed at supply air inlet.



Figure 20 Velocity at different position(a)Mouth breathing;(b)Nose breathing

As for supine position experiment, the supply air had 3 different velocities, 0.15m/s, 0.25m/s and 0.35m/s respectively. The velocity distributions were very similar with different breathing mode and different supply air velocity. However, when the magnitude of supply air was 0.15m/s, from 15cm vertical distance to 5cm vertical distance, the velocity increased slightly. This phenomenon present that the human thermal plume has interaction with supply air at this height, the direction of velocity at 5cm vertical distance from head is upward.



391



Figure 21 Turbulence intensity at different position(a)Mouth breathing;(b)Nose breathing

In these two figures, the impact of different breathing mode on turbulence intensity

was different. Considering the direction of the breathing jet in different breathing mode, the direction of mouth breathing airflow is more vertical. When the supply air velocity is low(0.15m/s), the impact of mouth breathing mode was smaller than nose breathing mode. At the 35cm vertical distance above the head, the mouth breathing air had made disturbance to the supply air, when the magnitude of velocity is 0.15m/s, this disturbance was the most prominent. Mouth breathing would distract the supply air.

As for nose breathing case, when the supply air velocity was 0.15m/s, because of the nose breathing jets, at the 15cm vertical distance from face, the turbulence intensity increased dramatically. However, when the supply air velocity was 0.25m/s or 0.35m/s, the turbulence intensity increased slightly.

402 3.2.3 Comparison between the simulation and experiment

For both sitting and supine posture, the velocity above the head from the CFD results were a little higher than the experimental data. In Fig.22, It was easy to observed that the supply air velocity did not reach the setting point in experimental study, that might cause the simulation results larger than the experiment data.

For sitting posture, the trend of these three lines were the same, but the simulation results were a little lower than experiment data in philtrum and forehead region. That might because the impact of breathing air jet was stronger in these region. Except for the supply air point, the difference between the CFD results and experiment data was less than 10%. For supine posture, the three line also had the same trend. The CFD results were more close to the nose breathing experimental data. The impact of



413 breathing mode was much more significant in supine posture.

Figure 22 Velocity comparison between simulation and experiment

(a)Sitting posture;(b)Supine posture

414

415 *3.3. air quality for the investigated cases*

416 The average contaminant exposure indices (ε_{exp}) and the intake fraction (*IF*)

417 were summarized for each group according to the location of the pollutant source.

418 3.3.1 Sitting position

With the increasing of the supply air velocity, the ε_{exp} value decreased 419 significantly no matter where the pollutant source was placed. The flow mode of the 420 inhalation and the exhalation of the manikin showed little influence on the ε_{exp} values. 421 When the supply air velocity was at 0.25m/s, the supply air could not deliver the 422 423 required fresh air to the BZ, and the pollutant concentration level in the BZ was almost the same with that at the exhaust, which means that a low supply air velocity is not 424 helpful for improving the air quality in the breathing zone, as it for the mixing 425 ventilation. 426



Figure 23 Contaminant exposure index(sitting) (a)case 1;(b)case 2;(c)case 3

As for the source placed in front of the manikin and near the manikin, when the supply air velocity was 0.30m/s, the ε_{exp} was significantly decreased, if increase the supply air velocity to 0.35m/s, the ε_{exp} could decrease lower than 0.25. Because these two source near manikin, increasing the supply air velocity had more efficiency to improve the air quality. When the pollutant source near the door, because of the distance from manikin to pollutant source was far, increasing the supply air velocity from 0.30m/s to 0.35m/s had less efficiency to improve the air quality.

435 The *IF* values show the same decreasing tendency with the increase of supply 436 velocity as for ε_{exp} values. Similarly, the mode of the inhalation and exhalation flow 437 of the manikin shows no influence on the *IF* values either.



Figure 24 Intake fraction(sitting) (a)case 1;(b)case 2;(c)case 3

438 3.3.2 Supine position

The same with sitting position cases, the *IF* values show the same decreasing tendency with the increase of supply velocity as for ε_{exp} values. According to the results obtained, contaminant exposure index ε_{exp} shows an decreasing tendency with the increase of supply velocity for all four cases investigated. With the increase of the supply air velocity, no matter where the pollutant source placed, the ε_{exp} value was significantly decreased. The mode of the inhalation and exhalation flow of the manikin shows no influence on the ε_{exp} values. When the supply air velocity was 0.15m/s, the supply air can only deliver a little fresh air to the breathing zone, the pollutant concentration in breathing zone was slightly lower than pollutant concentration in exhaust which means the low supply air only has little effect on improve the air quality in breathing zone.

450



Figure 25 Contaminant exposure index(lying) (a)case 4;(b)case 5

As for the supine position, when the supply air velocity increased to 0.25m/s, the ε_{exp} decreased quickly. If the supply air velocity increased to 0.30m/s from 0.25m/s, the ε_{exp} decreased slightly. It was the same with sitting position cases, however the supply air velocity had difference.

The *IF* values show the same decreasing tendency with the increase of supply velocity as for ε_{exp} values. Similarly, the mode of the inhalation and exhalation flow of the manikin shows no influence on the *IF* values either.



Figure 26 Intake fraction(lying) (a)case 4;(b)case 5

458 *3.4. Pollutant removal efficiency*

459 3.4.1 Sitting position

For the sitting position cases, when the supply air velocity increased to 0.30m/s, the E_{ff} reached over 82%, and even over 90% when the source was 1m in front of manikin. Although the ε_{exp} and *IF* were almost the same as that of the mixing ventilation system, the E_{ff} reached over 26% when the supply air velocity was at 0.25m/s. At 0.25m/s, the breathing mode and the position of the pollutant source were found to have much more significant influence on the E_{ff} compared to the other two experimented supply air velocities.









Figure 27 Pollutant removal efficiency (sitting) (a)case 1;(b)case 2;(c)case 3

468 When the supply air velocity increased from 0.30m/s to 0.35m/s, the E_{ff} 469 increased slightly. When the supply air velocity increased from 0.25m/s to 0.30m/s, the 470 E_{ff} increased dramatically. Compared to the 0.25m/s and 0.35m/s, the supply air 471 velocity set at 0.30m/s was the most suitable one.

472 3.4.2 Supine position

For the case of supine position, when the supply velocity air increased to 0.25m/s, the E_{ff} reached over 84%, and even over 90%. Although the ε_e and *IF* were almost the same as that of the mixing ventilation system, the E_{ff} was over 26% when the supply air velocity was 0.15m/s. At 0.15m/s, the breathing mode and the position of the pollutant source were found to have much more significant influence on the E_{ff} when compared to the other two supply air velocities. With an increased supply air velocity, the influence mitigated.

480



Figure 28 Pollutant removal efficiency(lying) (a)case 4;(b)case 5

When the supply air velocity increased from 0.25m/s to 0.35m/s, the E_{ff} slightly increased. However, the E_{ff} dramatically increased as the supply air velocity increased from 0.15m/s to 0.25m/s. Compared to when the supply air was 0.15m/s and 0.35m/s, 0.25m/s was found to be a better setting for pollutant removal.

485 3.5. Practical limitations

Although this study is unique in its design and could offer scientific evidence to support the potential realization of a new ventilation concept in bedroom, living room or ward of a hospital, it does suffer from some limitations. First, this study focused on the airborne contaminant and did not consider dynamic supply air temperature. Second, transient conditions that could influence the contaminant movement (e.g., door openings, and human movement) were also not taken into account.

492 **4.** Conclusion

This study presented detailed experimental and simulation results on the pollutantremoval efficiency of a localized laminar airflow system considering the impact

495 between respiratory activities and thermal plume. Localized laminar airflow system 496 manifested a special form of mixing ventilation through the use of supply panel with 497 small slot for direct breathing zone air delivery, to dilute the contaminated air in the 498 sub-zones.

The contaminant exposure index (ε_{exp}) and intake fraction (*IF*) results indicated the effectiveness of the proposed ventilation strategy. We found that the contaminant exposure of the manikin was highly dependent on the supply air velocity, especially when the supply air at the relatively low velocity levels. With an increased supply air velocity, the impact of the breathing mode on the exposure index (ε_{exp}), intake fraction (*IF*), and pollutant removal efficiency alleviated.

Positions of the pollutant sources showed little effect on the exposure risk and the intake fraction (*IF*) of the manikin, so did it on the E_{ff} . The results also showed that the exposure risk is significantly lower if choosing a suitable supply air velocity.

508 Localized laminar airflow system was proven to be an effective way of maintaining air cleanness in the BZ. According to ASHRAE 55, ISO 7730 and the 509 Chinese standard "Indoor air quality standard (GB/T 18883-2002)", with the modified 510 511 system on, the temperature around human body is in the comfort range. For sitting posture, the velocity is over 0.25m/s, which is a little higher than the comfort range, but 512 513 for supine posture, the velocity is in the comfort range. It means that, with the suitable 514 supply air velocity, the localized laminar airflow system would not influence the 515 thermal environment around human. This kind of system could be used in bedroom,

- 516 living room or any other kind of room which people only has low labour intensity
- 517 activities or they were in resting state.

518 5. Declarations

- 519 *5.1. Ethics approval and consent to participate*
- 520 Not applicable.
- 521 5.2. Consent for publication
- 522 Not applicable
- 523 5.3. Availability of data and materials
- 524 The datasets used and/or analysed during the current study are available from the
- 525 corresponding author on reasonable request.
- 526 5.4. Competing interests
- 527 The authors declare that they have no competing interests.
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535 5.6. Authors' contributions

Zhu Cheng and Amar Aganovic did the experiment and analyzed the data. Zhu
Cheng was the major contributor in writing the manuscript. Guangyu Cao provided
technical support and theoretic instruction. Zhongming Bu helped to complete the
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